FOCUS ON

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# Current state of the art approaches in Hepatobiliary Imaging

### HEPATOBILIARY MAGNETIC RESONANCE IMAGING

Magnetic Resonance Imaging (MRI) of the abdomen is the current gold-standard imaging modality in a wide array of pathologies that involve the upper abdominal organs. Up to a decade ago, it was very difficult to obtain good quality diagnostic images of any moving organ, including the liver. Continued technological advance has nowadays made it possible to image abdomen, and even organs with fast continuous motion such as the heart. MRI is a multiparametric exam - in that it is the only imaging modality that provides us with an array of different information; this is not only limited to 'enhancement' following administration of intravenous contrast (unlike CT). The additional information that is provided includes the intrinsic T1 and T2 signal of the tissue under study (Figure 1), sequences that show us the presence of macroscopic or intracellular fat, sequences that show us the degree of diffusion of water molecules (diffusion weighted imaging,



Figure 1: Magnetic resonance cholangiopancreatography (MRCP) is a special application of MRI. Images are heavily T2 weighted and fat-suppressed, this emphasises the pancreatico-biliary tree and suppresses the surrounding tissues. This MRCP shows the pancreaticobiliary tree in great detail. Note is made of multiple branch duct intraductal papillary mucinous neoplasms (IPMNs, arrowhead), precursor lesions at low risk of becoming pancreatic adenocarcinoma that need frequent monitoring by serial MRI. DWI), sequences that allow quantification of specific ions or macromolecules, and sequences that show us organ or lesion stiffness.

Two types of contrast agents can be used for abdominal MRI - extracellular contrast agents that travel within the vascular pool to be excreted by the kidneys, and hepatobiliary contrast agents (HBAs). HBAs are also gadolinium-based (like extracellular contrast agents), however they can be used for both dynamic vascular and hepatobiliary phase imaging given that around 50% of these contrast agents are taken up by hepatocytes with subsequent biliary excretion (hepatobiliary phase, Figure 2). The fraction taken up by hepatocytes produces a notable prolonged increase in liver signal intensity with minimal or no enhancement of non-hepatocellular lesions.

DWI relies on imaging motion of water molecules. Free water molecules are in constant random motion (Brownian motion). Motion of water molecules within the cellular microenvironment is impeded by their interaction with cellular compartments, including the hydrophobic cell membrane and intracellular organelles. Restriction in the diffusion of water molecules is therefore directly proportional to the degree of cellularity of the tissue. Most malignancies are hypercellular relative to the surrounding tissue - restricting Brownian motion, and thereby diffusion (Figure 3).

## CONTRAST ENHANCED ULTRASOUND (CEUS)

Contrast ultrasound relies on the use of microbubbles that are small enough to cross capillary beds (< 7µm). Such microbubbles need to be stable enough to endure cardio-pulmonary transit before ending in the systemic circulation. They also need to be stable enough to endure the low-energy ultrasound beam for the time required to reach a diagnosis. Microbubbles react to the alternating compression and rarefaction of sound waves in the ultrasound beam. They halve in size during compression and double in size during rarefaction. This results in a strong reflected signal, allowing us to visualize individual microbubbles even though the mean diameter of microbubbles is 2.5µm. The most widely available agent in Europe was approved in 2001 and consists of Sulphur Hexafluoride (SF6) stabilised in a



Figure 2: Patient with a persistent bile leak post-cholecystectomy. MRI using hepatobiliary contrast agents was performed in order to identify site of the leak. Leakage from the cystic duct stump is seen (arrowhead), together with layering of contrast around the liver. Patient had endoscopic stenting, with resolution of the bile leak and excellent recovery.



Figure 3: Solitary colorectal metastatic deposit seen on both DWI MRI (red arrowhead), contrast ultrasound (blue arrowhead), and conventional ultrasound (white arrowhead). DWI shows restricted diffusion, with the lesion being more conspicuous on the heavily diffusion weighted image (b=800) as compared to the other images (b=0, 50, 400).

phospholipid monolayer membrane. Microbubbles are excreted via the lungs, allowing safe use in patients with renal failure. CEUS is useful in a wide variety of clinical scenarios (Figures 3 and 4). Contraindications are rare, and include a recent acute coronary syndrome, clinically unstable ischaemic heart disease, known significant right-to-left shunts, severe pulmonary hypertension, uncontrolled systemic hypertension, and acute respiratory distress syndrome. Safety has not yet been established in pregnancy and lactation.

# ELASTOGRAPHY

Chronic liver disease is becoming more and more common in the developed world. This is mostly due to the increased prevalence of non-alcoholic liver disease (NAFLD). Clinical, radiological, and biochemical features point to established cirrhosis, but not earlier potentially reversible fibrosis. Fibrosis is a response to chronic liver injury and is thought to be mediated by hepatic stellate cells (myofibroblasts), located in the perisinusoidal space (space of Disse). Accurate detection and intervention at the earlier stages of fibrosis has the potential to reduce morbidity and prevent end-stage disease, since early fibrosis is potentially reversible.

From a physics point of view, elastography aims to image the Young's E modulus, which measures the force (per unit area) that is needed to stretch (or compress) a material sample. All elastography techniques rely on the same basis: an external force is applied to the studied tissue and the resulting movements are then followed.

Traditionally, the presence and grading of fibrosis was achieved through image-guided percutaneous liver biopsy (PLB). This has been considered as being the gold standard for the past 50 years despite numerous advantages, including the invasive nature of a biopsy (not an ideal test to keep monitoring disease in the same patient; however risk of serious complications is low), sampling variability (especially important since the specimen obtained represents less than 1/50,000 of liver),<sup>3</sup> and high interobserver variability during microscopic evaluation.<sup>2</sup>

Elastography can be performed using both ultrasound and MRI. In both cases shear waves are generated in tissues following the application of a directional force



Figure 4: CEUS showing a multilocular pyogenic liver abscess straddling the middle hepatic vein (arrowhead), in a young patient with diabetic ketoacidosis. This was not visible on conventional ultrasound.



Figure 5: Two different patients who underwent 2D-SWE. Colorcoded images depict tissue stiffness in both cases, with the propagation map to the right. The lines of the propagation map are parallel, confirming that the measurements taken are reliable.

Normal elasticity is seen in a young healthy female (Patient 1). Contrasting images are seen at the bottom in a mid-aged male with nonalcoholic steatohepatitis cirrhosis, with evident increased stiffness (Patient 2) and increased interval between consecutive lines of the propagation map.

which causes shear deformation. One of the most extensively studied approaches in ultrasound is 'point' shear wave elastography (SWE) via acoustic radiation force imaging (ARFI).<sup>3</sup> The force produced slightly displaces the tissue at the focal spot according to Hooke's law. Following this, the transducer switches into imaging mode to detect displacements of the focal spot by tracking of the ultrasound signal (called "speckle"). This identifies the displacement of tissue with sensitivity of less than a micrometer. ARFI elastography is very accurate - with areas under the curve ranging from 0.848 to 0.862 when compared to actual liver biopsies.<sup>4</sup>

Another ultrasound-based approach is two-dimensional (2D) SWE (Figure 5), in which the elasticity profile of a larger section of tissue is evaluated. Here shear wave arrival times (or "wavefronts") at different locations are plotted, allowing a 2D map of shear wave properties within a section of liver to be generated. Some manufacturers also display a propagation map, with contour lines to depict shear wave arrival times at different points in the tissues, in order to guide optimal sampling.

MRI elastography (MRE) is accomplished in 3 steps: generation of mechanical shear waves in tissue by an acoustic driver, imaging of these shear waves with a special MRI sequence, and processing of the wave information to generate elastograms.<sup>5</sup> The volume of liver parenchyma assessed with a single slice of MRE is about 250cm<sup>3</sup>. This is much higher than point shear wave elastography (0.5-1.0cm<sup>3</sup>), and nearly 500 times that of a liver biopsy (10-50mm<sup>3</sup>).<sup>6</sup> MRE can show heterogeneous involvement of the liver in fibrosis (Figure 6), and is usually feasible in most patients (obese, bowel interposition, ascites). However, the most important advantage when compared to ultrasound-based methods lies in its high reliability in diagnosing fibrosis in significantly obese patients, a major limitation in ultrasound.

Confounding factors that might decrease the accuracy of elastography include postprandial condition (patients must be fasted for at least 3 hours prior to elastography), elevated aminotransferases to more than 5x the upper limit of normal in the context of necroinflammation (seen in acute hepatitis or acute liver failure), right heart failure, and cholestasis.



Figure 6: Conventional CT images show hepatomegaly in a patient with NAFLD. No evidence of cirrhosis on CT. MRE (bottom right image) shows patchy increased liver stiffness (seen in green, yellow, and red) compatible with established cirrhosis despite normal appearances in CT.

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